

according to the present disclosure, three-dimensional sample manipulation is possible, including rotation in addition to linear transport. In the context of RF detection and imaging discussed in greater detail below, the vertical microcoil may allow large-signal RF perturbations for imaging, while the planar microcoil provides a DC field to manipulate the samples, thereby enhancing the capability of a hybrid system incorporating both vertical and planar microcoils.

[0123] Having discussed various aspects of the structure and fabrication of an exemplary microcoil according to the present disclosure based on conventional semiconductor fabrication processes, the interaction between neighboring microcoils in an array with respect to the generation of magnetic fields for sample manipulation is now considered in greater detail. As discussed above, the principle of operation of the microcoil array 200B shown in FIGS. 6(a) and (b) is to create and move one or more magnetic field peaks by modulating currents in the respective microcoils 212 of the array so as to move and/or trap magnetic samples. The magnitude of the magnetic field generated by a given microcoil of the array is based on the magnitude of the current flowing through the microcoil, and each microcoil in the array is capable of generating a local magnetic field peak above the microcoil. In this sense, the array 200B may be thought of generally in terms of “magnetic pixels,” wherein an N×N array of microcoils is capable of producing at least N×N magnetic peaks, or “pixels,” each capable of attracting and trapping a sample. FIG. 10 conceptually illustrates two neighboring microcoils 212-1 and 212-2 of the array 200B, in which an essentially equal current 230 flows through the microcoils to generate two essentially equal magnetic field peaks 232-1 and 232-2 above the coils. In FIG. 10, the distance between the two magnetic field peaks generally corresponds to the pitch 216 of the array 200B, as indicated in FIGS. 6(a) and 10.

[0124] In one embodiment, not only may the magnitude of the current flowing through each microcoil be modulated to facilitate sample manipulation, but also the direction of the current flowing through a given coil may be altered, so as to facilitate a smoother transition of a sample from pixel to pixel, or effectively increase the spatial resolution for sample manipulation (i.e., effectively decrease the pitch 216 of the array). FIGS. 11(a)-(e) show five exemplary scenarios for the neighboring microcoils 212-1 and 212-2 of FIG. 10, with varying current magnitudes and directions in the respective coils and the resulting magnetic fields generated. FIG. 12 is a graph illustrating the current magnitude and direction in each of the coils for each of the five exemplary scenarios illustrated in FIGS. 1 I(a)-(e). On the horizontal axis of FIG. 12, the steps 1-5 correspond respectively to the five scenarios illustrated in FIGS. 11(a)-(e). The upper plot shown on the graph of FIG. 12 indicates the current 230-1 flowing through the “left” microcoil 212-1 in each scenario, and the lower plot indicates the current 230-2 flowing through the “right” microcoil 212-2 in each scenario.

[0125] In particular, in FIG. 11(a), as indicated in step 1 of the graph of FIG. 12, the left microcoil 212-1 has no current flowing through it, while the right microcoil 212-2 has -20 mA of current flowing through it. As a result, a magnetic field peak 232-2 is generated above the right microcoil 212-2. In one exemplary implementation based on the microcoil structure discussed above in connection with FIGS. 7-9, the magnitude of the magnetic field peak 232-2

thus generated may be on the order of approximately 30 Gauss. In FIG. 11(b), as indicated in step 2 of FIG. 12, the current 230-1 in the left microcoil is increased to approximately 12-13 mA, while the current 230-2 in the right microcoil is decreased to approximately -19 mA. As shown in FIG. 11(b), the magnetic field starts to broaden somewhat above the two microcoils, as there is now some field contribution from both the left and right microcoils.

[0126] In FIG. 11(c), as indicated in step 3 of FIG. 12, the left and right microcoils have equal magnitude currents flowing through them (approximately 17-18 mA), but in opposite directions; as a result, a broad magnetic field peak is generated, roughly centered over the midpoint between the centers of the respective coils. In FIG. 11(d), the current 230-1 is further increased in the left microcoil 212-1 and the current 230-2 is further decreased in the right microcoil 212-2, and in FIG. 11(e) the current 230-1 ultimately is increased to 20 mA while the current 230-2 ultimately is reduced to zero; as a result, a single magnetic field peak 232-1 is maintained over the left microcoil 212-1. It should be appreciated that the respective fields generated in FIGS. 11(a) and 11(e) have the same magnitude, but opposite field directions. Accordingly, by gradually varying currents of different directions through the coils, a magnetic field peak may be continuously moved between two adjacent coils, thus effectively enhancing the resolution of the array to facilitate precise positioning as well as smooth translation of samples across the array 200B.

[0127] As discussed above in connection with FIGS. 1 and 2, in one embodiment various field control components 400 for controlling and distributing current (and/or voltage) to the microcoils of the array 200B may be integrated together with the array in an IC chip 102. In one exemplary implementation, these field control components include one or more current sources (and/or voltage sources), as well as various switching or multiplexing components to facilitate digital (and computer programmable) control of the fields generated by the array 200B.

[0128] FIG. 13 is a diagram showing the microcoil array 200B and various field control components associated with the array 200B, according to one embodiment of the present disclosure. In the example of FIG. 13, the array 200B includes eight rows and eight columns of “microcoil cells” 250, wherein each microcoil cell includes a microcoil 212, as well as switches and logic circuits, as discussed further below in connection with FIGS. 14 and 15. For purposes of distributing current (and/or voltage) to the microcoil cells 250, the array 200B of this embodiment is divided into four quadrants 200B-1, 200B-2, 200B-3 and 200B-4, each quadrant having sixteen microcoil cells 250 (i.e., four rows and four columns per quadrant). It should be appreciated, however, that microcoil arrays and associated control components according to the present disclosure are not limited in this respect, and that the particular configuration shown in FIG. 13 is provided primarily for purposes of illustration.

[0129] As shown in FIG. 13, the various field control components associated with the array 200B in this embodiment include a row decoder 460-1 that provides row enable signals R0-R7 to respective rows of the array 200B, and a column decoder 460-2 that provides column enable signals C0-C7 to respective columns of the array. The row decoder