

**160**, which is defined at the first end **142** of the microfluidic device **140**, is therefore formed above the planar surface **126**.

[0045] The second end **144** of the microfluidic channel **140** is formed in a protrusion **170** that extends outwardly from the second face **130**. As with the prior embodiment, the protrusion **170** preferably has a tapered shape (inward taper) such that it forms a generally conical structure with the open second end **144** being formed at an apex of the conical structure. The tapered protrusion **170** therefore acts as a nozzle that can discharge a sample that is loaded into the microfluidic channel **140** (e.g., in the reservoir **160**). The nozzle **170** is therefore part of the microfluidic channel structure since the microfluidic channel **140** is formed therethrough and terminates at the nozzle opening.

[0046] The second face **130** is also not substantially planar but rather includes a second perimeter wall **132** that extends at least partially around a perimeter of the second face **130**. The second face **130** does contain a floor **134** that is substantially planar. Between the second perimeter wall **132**, one or more nozzle base sections **180** are formed with the number of nozzle base sections **180** being equal to the number of microfluidic channels **140**. The nozzle base sections **180** are integrally formed with and extend outwardly from the floor **134** and in the illustrated embodiment, each nozzle base section **180** has a generally annular shape. However, the shape of the nozzle base section **180** is not limited to an annular shape and instead can have any number of shapes, including a conical shape or a tapered shape or any other regular or irregular shape. According to one embodiment, a plane that contains the upper edge of the second perimeter wall **132** generally cuts through the interface between the nozzle base section **180** and the nozzle **170**. The nozzle **170** therefore extends beyond the upper edge of the second perimeter wall **132**. According to one embodiment, the diameter of the reservoir **160** is about equal to the outside diameter of the nozzle base section **180**; and therefore, an outside diameter of the reservoir wall **124** is greater than the outside diameter of the nozzle base section **180**.

[0047] The specific configurations of the nozzle **170** and the microfluidic channel **140** are best shown in FIG. 5. As illustrated, the first end **142** of the microfluidic channel **140** is in the form of the reservoir **160**. A distal end of the reservoir **160** has an inwardly tapered construction that leads to an intermediate channel section **146**. A substantial length of the intermediate channel section **146** is formed in the nozzle base section **180**. The intermediate channel section **146** also has a tapered construction in that it tapers inwardly toward the nozzle **170** defined at the second end **144** of the microfluidic channel **140**. Thus, the dimensions of the microfluidic channel **140** are greatest at the first end **142** and are at a minimum at a tip portion **172** of the nozzle **170**. In one embodiment, the microfluidic feature formed in the device **100** beginning with the reservoir **160** and terminating with the nozzle **170** is generally cylindrical in shape along its length. According to one exemplary embodiment, the open second end **144** of the microfluidic channel **140** formed at the tip portion **172** has an inside diameter equal to or less than  $100\ \mu\text{m}$ , preferably equal to or less than  $50\ \mu\text{m}$  and more preferably, equal to or less than  $20\ \mu\text{m}$ ; and an outside diameter of the nozzle, as measured at a tip portion thereof, is less than about  $150\ \mu\text{m}$  and preferably is equal to or less than about  $100\ \mu\text{m}$ , and more preferably equal to or less than

$50\ \mu\text{m}$ . The inside diameter of the microfluidic channel **140** varies along its length due to its tapered construction. For example, the inside diameter of the microfluidic channel **140** opens gradually in a direction away from the nozzle **170** to about several hundred  $\mu\text{m}$  as the microfluidic channel **140** traverses through the thickness of the substrate body **110** and eventually, the microfluidic channel **140** is formed to a diameter of about  $1.5\ \text{mm}$  to define the reservoir **160**. The length of the microfluidic channel **140** can be tailored in view of the construction details of the microfluidic device **100** and the potential applications of the device **100**. In one example, the length of the microfluidic channel **140** is about  $3\ \text{mm}$ ; however, this will vary depending upon the thickness of the device **100**, the amount of sample that is to be loaded into the device, etc.

[0048] As with the first embodiment, the microfluidic channel **140** is formed in a substantially perpendicular manner in the substrate body **110** since the microfluidic channel **140** is formed substantially perpendicular to both the first and second faces **120**, **130**. While, the nozzle **170** extends beyond a plane containing the distal edge of the second perimeter wall **132**, the distal end of the reservoir wall **124** preferably lies within the same plane that contains the distal edge of the first perimeter wall **122**. This orientation permits a cover (e.g., thin polymeric cover sheet) or seal member to be disposed across the distal edge of the first perimeter wall **122** and the distal ends of the reservoir wall **124** to effectively seal the sample material within the reservoir **160**, as will be described hereinafter.

[0049] One will appreciate that one of the advantages of the device **100** is that it is formed as a one piece construction in contrast to conventional devices which have multiple layers bonded together. In these conventional devices, the microfluidic channel is closed by the bonding of one layer over another layer. In other words, two separate layers are needed to define the complete channel. Because the present device **100** is injection-molded, separate bonded layers are not required.

[0050] It will be understood that the present configurations that are illustrated herein with reference to FIGS. 1-5 are merely exemplary in nature and are intended to merely convey exemplary embodiments. Various modifications can be performed to the microfluidic devices depending upon a number of different considerations, including manufacturing considerations. For example, the nozzle structures do not necessarily have to have conical shapes; however, for ease of manufacturing, a conical shape or the like is generally preferred.

[0051] According to another aspect of the present application, various manufacturing methods are disclosed herein for manufacturing the microfluidic array devices illustrated in FIGS. 1-5. In general terms, exemplary manufacturing processes disclosed herein permit microfluidic nozzle array devices to be manufactured having microscale nozzle dimensions (e.g., a nozzle tip opening having a diameter equal to or less than  $100\ \mu\text{m}$ , preferably equal to or less than  $50\ \mu\text{m}$  and more preferably, equal to or less than  $20\ \mu\text{m}$ ; and an outside diameter of the nozzle, as measured at a tip portion thereof, is less than about  $150\ \mu\text{m}$  and preferably is equal to or less than about  $100\ \mu\text{m}$ , and more preferably equal to or less than  $50\ \mu\text{m}$ ) and also the present microfluidic array devices are particularly suited to inexpensive fabrica-